

Manuscript Details

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Title	Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of Cervical Multifidus Muscle in Healthy People: Imaging Capturing and Imaging Calculation
Article type	Technical & measurement reports

Abstract

Background: Studies have analyzed muscle morphometry of cervical multifidus by using ultrasound imaging, but its reliability is not clearly determined. Objective: To investigate intra- and inter-rater reliability of imaging capturing (probe assessment/patient positioning) and imaging calculation (scan assessment) of cervical multifidus cross sectional area (CSA) by considering the assessor's experience in asymptomatic individuals. Design: Reliability study. Methods: The CSA of C4/C5 cervical multifidus was assessed in 16 asymptomatic subjects. Two examiners performed the imaging capture and also repeated the procedure (probe placement/patient positioning) twice with a 10-min period between each. Other two raters conducted imaging calculations of CSA. Intra-examiner imaging capturing reliability, each rater (experienced and novice) calculated multifidus CSA of both images obtained by each examiner. Inter-examiner imaging capturing reliability, each rater calculated the CSA obtained by each examiner at the first imaging attempt. For imaging calculation reliability, each rater calculated multifidus CSA of all images captured by both examiners. Intra-class correlation coefficients (ICC) and standard error of measurement (SEM) were calculated. Results: Intra- (ICC3,1 0.988-0.996, SEM 0.3%-0.7%) and inter- (ICC3,2 0.958-0.965, SEM 2.6%-3.2%) examiner reliability of imaging capturing was excellent. Intra- and inter-rater reliability of imaging calculation was also excellent for both raters (experienced/novice). No significant differences between experienced or novice examiners or testers were found. Conclusions: This study found that intra- and inter-examiner/rater reliability of imaging capturing (probe assessment/patient positioning) and imaging calculation (scan assessment) of the cervical multifidus CSA at C4/C5 level was excellent in asymptomatic subjects.

Keywords	Rehabilitative ultrasound imaging; cervical multifidus; reliability.
Taxonomy	Medicine, Medical Specialty
Corresponding Author	César Fernández-de-las-Peñas
Corresponding Author's Institution	Aalborg University
Order of Authors	Juan Antonio Valera-Calero, Sandra Sánchez-Jorge, Javier Alvarez-González, Ricardo Ortega, Josh Cleland, César Fernández-de-las-Peñas, José Luis Arias-Buría
Suggested reviewers	Maria Stokes, Emilio Puentedura, Carol A Courtney

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STARD 2015

AIM

STARD stands for “Standards for Reporting Diagnostic accuracy studies”. This list of items was developed to contribute to the completeness and transparency of reporting of diagnostic accuracy studies. Authors can use the list to write informative study reports. Editors and peer-reviewers can use it to evaluate whether the information has been included in manuscripts submitted for publication.

EXPLANATION

A **diagnostic accuracy study** evaluates the ability of one or more medical tests to correctly classify study participants as having a **target condition**. This can be a disease, a disease stage, response or benefit from therapy, or an event or condition in the future. A medical test can be an imaging procedure, a laboratory test, elements from history and physical examination, a combination of these, or any other method for collecting information about the current health status of a patient.

The test whose accuracy is evaluated is called **index test**. A study can evaluate the accuracy of one or more index tests. Evaluating the ability of a medical test to correctly classify patients is typically done by comparing the distribution of the index test results with those of the **reference standard**. The reference standard is the best available method for establishing the presence or absence of the target condition. An accuracy study can rely on one or more reference standards.

If test results are categorized as either positive or negative, the cross tabulation of the index test results against those of the reference standard can be used to estimate the **sensitivity** of the index test (the proportion of participants *with* the target condition who have a positive index test), and its **specificity** (the proportion *without* the target condition who have a negative index test). From this cross tabulation (sometimes referred to as the contingency or “2x2” table), several other accuracy statistics can be estimated, such as the positive and negative **predictive values** of the test. Confidence intervals around estimates of accuracy can then be calculated to quantify the statistical **precision** of the measurements.

If the index test results can take more than two values, categorization of test results as positive or negative requires a **test positivity cut-off**. When multiple such cut-offs can be defined, authors can report a receiver operating characteristic (ROC) curve which graphically represents the combination of sensitivity and specificity for each possible test positivity cut-off. The **area under the ROC curve** informs in a single numerical value about the overall diagnostic accuracy of the index test.

The **intended use** of a medical test can be diagnosis, screening, staging, monitoring, surveillance, prediction or prognosis. The **clinical role** of a test explains its position relative to existing tests in the clinical pathway. A replacement test, for example, replaces an existing test. A triage test is used before an existing test; an add-on test is used after an existing test.

Besides diagnostic accuracy, several other outcomes and statistics may be relevant in the evaluation of medical tests. Medical tests can also be used to classify patients for purposes other than diagnosis, such as staging or prognosis. The STARD list was not explicitly developed for these other outcomes, statistics, and study types, although most STARD items would still apply.

DEVELOPMENT

This STARD list was released in 2015. The 30 items were identified by an international expert group of methodologists, researchers, and editors. The guiding principle in the development of STARD was to select items that, when reported, would help readers to judge the potential for bias in the study, to appraise the applicability of the study findings and the validity of conclusions and recommendations. The list represents an update of the first version, which was published in 2003.

More information can be found on <http://www.equator-network.org/reporting-guidelines/stard>.



1 Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of
2 Cervical Multifidus Muscle in Healthy People: Imaging Capturing and
3 Imaging Calculation
4

5 **Abstract**

6 **Background:** Studies have analyzed muscle morphometry of cervical multifidus by using
7 ultrasound imaging, but its reliability is not clearly determined. **Objective:** To investigate
8 intra- and inter-rater reliability of imaging capturing (probe assessment/patient positioning)
9 and imaging calculation (scan assessment) of cervical multifidus cross sectional area (CSA)
10 by considering the assessor's experience in asymptomatic individuals. **Design:** Reliability
11 study. **Methods:** The CSA of C4/C5 cervical multifidus was assessed in 16 asymptomatic
12 subjects. Two examiners performed the imaging capture and also repeated the procedure
13 (probe placement/patient positioning) twice with a 10-min period between each. Other two
14 raters conducted imaging calculations of CSA. Intra-examiner imaging capturing reliability,
15 each rater (experienced and novice) calculated multifidus CSA of both images obtained by
16 each examiner. Inter-examiner imaging capturing reliability, each rater calculated the CSA
17 obtained by each examiner at the first imaging attempt. For imaging calculation reliability,
18 each rater calculated multifidus CSA of all images captured by both examiners. Intra-class
19 correlation coefficients (ICC) and standard error of measurement (SEM) were calculated.
20 **Results:** Intra- (ICC_{3,1} 0.988-0.996, SEM 0.3%-0.7%) and inter- (ICC_{3,2} 0.958-0.965, SEM
21 2.6%-3.2%) examiner reliability of imaging capturing was excellent. Intra- and inter-rater
22 reliability of imaging calculation was also excellent for both raters (experienced/novice).
23 No significant differences between experienced or novice examiners or testers were found.

24 **Conclusions:** This study found that intra- and inter-examiner/rater reliability of imaging
25 capturing (probe assessment/patient positioning) and imaging calculation (scan assessment)
26 of the cervical multifidus CSA at C4/C5 level was excellent in asymptomatic subjects.

27 **Key words:** Rehabilitative ultrasound imaging, cervical multifidus, reliability.

29 **Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound**
30 **Imaging of Cervical Multifidus Muscle in Healthy People: Imaging**
31 **Capturing and Imaging Calculation**
32

33 **Introduction**

34 Mechanical neck pain of insidious onset and whiplash associated disorders (WAD)
35 represent a major health care problem. While the general prognosis of neck pain is positive,
36 up to 50% of individuals continue reporting symptoms after 1-year (Kamper et al, 2008).
37 There is no consensus regarding the potential pathophysiology of neck disorders. One
38 mechanism may be related to the fact that neck pain induces changes in cervical muscle
39 performance. Several studies have reported that people with WAD show increased fatty
40 infiltrate and changes in cross sectional area (CSA) in the posterior cervical muscles,
41 specifically the multifidi (Abbott et al, 2015; Elliot et al, 2014; Snodgrass et al, 2019a).
42 However, most studies have used magnetic resonance imaging (MRI) to assess muscle
43 morphology (Owers et al, 2018), which is not readily available in clinical practice.

44 A more pragmatic method of measuring muscle morphology is ultrasonography; but
45 it its reliability must first be demonstrated (Whittaker et al, 2017). Some studies have
46 investigated the reliability of rehabilitative ultrasound imaging (RUSI) for examination of
47 the posterior neck muscles (Javanshir et al, 2010). Kristjansson (2004) analyzed the
48 reliability of assessing CSA of the C4 cervical multifidus and reported appropriate intra-
49 and inter-tester agreement in 10 asymptomatic subjects, and acceptable intra-, but
50 questionable inter-tester, agreement in 10 symptomatic subjects. Fernández-de-las-Peñas et
51 al (2008) reported excellent between-scan and good between-day assessment in individuals
52 with mechanical neck pain. Lee et al (2007) found that ultrasound imaging was as reliable
53 and valid as MRI for assessing cervical multifidus thickness after isometric contractions.

54 An important step before neck muscle composition can routinely be used in research
55 or clinical practice is establishing reliability of imaging calculation (scan assessment) but
56 also reliability of imaging capturing (patient positioning). This is particularly relevant since
57 ultrasonography is operator-dependent and the measurement protocol could influence the
58 imaging calculation. In fact, previous studies had mostly investigated the reliability of
59 imaging calculation (scan assessment) but not the reliability of imaging capturing (probe
60 assessment /patient repositioning). Further, reliability according to the experience of the
61 assessor has not been properly investigated. Our aim was to determine intra- and inter-
62 examiner/rater reliability of imaging calculation (scan/image assessment) and imaging
63 capturing (probe assessment/patient positioning) of cervical multifidus CSA considering
64 assessor experience

65

66 **Methods**

67 **Participants**

68 Asymptomatic volunteers without neck pain symptoms were recruited via local
69 announcements between December 2018 and June 2019. To be eligible to participate, they
70 had to be between 18 and 45 years old and with no history of neck pain the previous year.
71 Exclusion criteria included history of whiplash injury; any pharmacological treatment
72 affecting muscle tone, e.g., muscle relaxants, analgesics; prior history of cervical surgery;
73 cervical radiculopathy or myelopathy; presence of degenerative changes; and any medical
74 condition such as tumor or fracture. The study was approved by the Institutional Review
75 Ethical Committee of XX. All subjects signed the written informed consent prior to their
76 inclusion.

77 **Procedure Assessment - Imaging Capturing**

78 All images were acquired with a Toshiba Xario® 100 ultrasound equipment with a
79 PLU-1005 BT (7-15MHz) linear probe. Gain, frequency, depth, or focus were pragmatically
80 adapted by the examiner for each exam. Participants were placed in a prone position with
81 their arms in 90° abduction and the elbows flexed to 90°. The head/neck were stabilized
82 using the plinth's facial hole. A passive cranio-cervical flexion movement was performed
83 by the examiner to achieve a neutral position of the neck/head.

84 It has been estimated that measurements of C4 would exhibit less error (Lee et al,
85 2007); therefore, we assessed C4/C5 multifidus. To identify the cervical multifidus level,
86 the C2 spinous process was identified by palpation. At that point, the US probe was moved
87 caudally two segments until the posterior arch of C4 vertebra was visually identified. Then,
88 the transducer was moved lateral over the articular pillar (**Fig. 1A**). The image (scan) was
89 captured when the most superficial point of the spinous tubercle cortical surface and the
90 most superficial point of C4/C5 joint were visualized simultaneously (**Fig. 1B**).

91 **Measurement Assessment - Imaging Calculation**

92 Once the US image was captured, it was transferred to offline Oxyiri® Software for
93 calculating the CSA of the cervical multifidus by using on-screen calipers traced around the
94 following contours: 1, inferior limit: internal echogenic fascia between cervical multifidus
95 and rotator muscle (deep to cervical multifidus); 2, superior limit: echogenic fascia between
96 cervical multifidus and semispinalis; 3, medial limit: echogenic spinous process (**Fig. 2**).

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101 **Examiners**

102 A total of 4 examiners participated in the study. For imaging capturing, one experienced
103 (10 years of practice) and one novice (1 year of practice) examiner performed the patient
104 positioning/procedure placement and captured two images of the posterior neck muscles as
105 described. Each examiner repeated the assessment, twice with a 10-min period between.
106 Participants were repositioned on each assessment. On each assessment, an image of the
107 posterior neck muscles was obtained (Fig. 1B).

108 Another two examiners, identified in our study as raters, again one experienced and
109 the second novice (same experience as examiners) participated in the imaging calculation
110 of all images. Every image was coded to blind raters using alphanumeric codes. The order
111 of assessment and raters was numerically randomized between participants.

112 **Reliability Calculations**

113 We assessed the reliability of both imaging capturing and imaging calculation by
114 considering the examiner/rater experience. For imaging capturing intra-examiner reliability,
115 each rater (experienced/novice) calculated CSA of both images obtained by each examiner
116 (experienced/novice) at both assessments. For imaging capturing inter-examiner reliability,
117 each rater (experienced/novice) calculated the CSA of the image captured by each examiner
118 (experienced/novice) at the first positioning assessment.

119 For imaging calculation intra-rater reliability, each rater (experienced/novice) determined
120 the CSA of all images obtained by both examiners twice, one-week apart. For imaging
121 calculation inter-rater reliability, each rater (experienced/novice) calculated the CSA of all
122 images obtained by both examiners once.

123

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125 **Statistical Analysis**

126 Statistical analysis was performed using the SPSS package, Version 21 software for
127 Mac OS. Normal distribution of the data was verified by using the Shapiro-Wilk test. Intra-
128 and inter- examiner/rater reliability was estimated using 2-way mixed-model, consistency-
129 type intra class correlation coefficients (ICC). Reliability was classified as fair (ICC<0.50),
130 moderate (0.50<ICC<0.75), good (0.75<ICC<0.90) or excellent (ICC>0.90) (Koo and Li
131 2016). Standard error of measurement (SEM) was calculated using the resulting ICC values
132 and standard deviation (SD): $SEM (\%) = (SD \times \sqrt{1-ICC}) \times 100$ to assess measurement precision.
133 All tests were two-tailed with p-values <0.05 considered significant.

134

135 **Results**

136 From a total of 20 subjects responding to the announcement, 4 were excluded due to
137 previous whiplash injury (n=2) and history of neck pain the previous year (n=2). Sixteen
138 asymptomatic subjects (50% male) were finally included (total 64 images, n=4 per subject).
139 **Table 1** provides demographic features. Male exhibited higher anthropometric outcomes
140 and larger CSA than female (P<0.001). A positive correlation between multifidus CSA and
141 weight (r:0.473, P=0.006), height (r:0.385; P=0.03), and BMI (r:0.481, P=0.005) was found.

142 **Table 2** shows reliability data of imaging capturing. In general, imaging capturing
143 intra-examiner reliability (ICC_{3,1}) was excellent ranging from 0.988 to 0.996 with a SEM
144 from 0.3% to 0.7%. No difference between experienced/novice examiner/testers was found.
145 Inter-examiner reliability was also excellent for both experienced (ICC_{3,2} 0.965) and novice
146 (ICC_{3,2} 0.958) raters, with SEM of 2.6% and 3.2%, respectively.

147 Reliability data of imaging calculation of both raters is shown on **Table 3**. Again,
148 intra- and inter-rater reliability was excellent for both raters but with smaller SEM for intra-
149 rater reliability.

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151 **Discussion**

152 This is the first study assessing reliability of both imaging capturing (positioning)
153 and imaging calculation (assessment) of the neck muscles considering the experience of the
154 assessor. In general, intra- and inter- rater reliability of imaging capturing and calculation
155 of cervical multifidus CSA was excellent when applied by an experienced or novice
156 assessor in asymptomatic individuals. Our findings are similar to those previously found in
157 patients with mechanical neck pain (Fernández-de-las-Peñas et al, 2008) and slightly better
158 than those previously reported by Kristjansson (2004). In addition, reliability data of
159 ultrasound imaging assessment was slightly superior to reliability data obtained for MRI.
160 Snodgrass et al (2019b) reported good to excellent intra- (ICC 0.78-0.96), but fair to good
161 inter- (ICC 0.44-0.88) rater reliability of cervical multifidus assessment using MRI in 5
162 asymptomatic individuals. Interestingly, no differences between an experienced and novice
163 examiner/rater were observed. This is a relevant topic since ultrasound imaging assessment
164 is operator-dependent. Two points are relevant for ultrasound assessment, probe angulation
165 and pressure. Whittaker et al (2009) showed that probe angulation of less than approx. 10
166 degrees, as it is commonly done in clinical practice, do not distort measurements of tissue
167 thickness. No data about probe pressure is available. It is possible that strict positioning and
168 measurement protocols followed in our study could explain high reliability values.

169 This study can help for developing specific protocols for image capturing and calculation
170 for both research and clinical practice. For instance, morphometry assessment, i.e., CSA, is
171 based on anatomical surrounding muscle contours. Previous studies recognized that lack of
172 proper visualization of the fascial layers dividing the cervical multifidus from surrounding
173 muscles (Fernández-de-las-Peñas et al, 2008; Kristjansson, 2004; Lee et al, 2007). One
174 potential reason for this lack of clarity of muscular fascial layers could be the presence of
175 fatty infiltration, a sign potentially associated with WAD (Owers et al, 2018). In the current
176 study, we assessed cervical multifidus, without including the rotators, as it was conducted
177 in previous studies (Fernández-de-las-Peñas et al, 2008; Kristjansson, 2004; Lee et al,
178 2007). The main reason was that the cervical multifidus attaches to the posterior aspect of
179 the facet capsules (Anderson et al, 2005) and play a relevant role in proprioception. In such
180 a scenario, fascial layers as border contours for determining muscle morphology may have
181 highly relevance. Since the current study included asymptomatic individuals, fascial layers
182 surrounding the multifidus were properly identified (Fig. 2). Rankin et al (2005) were not
183 able to consistently identify fascial divisions between multifidus/semispinalis and between
184 multifidus/rotators; therefore, they provided normative data of the whole muscle group and
185 not from individual muscles. It is also possible that technical improvements of ultrasound
186 imaging equipment, offering much better-definition and quality images, can also influence
187 proper visualization of fascial layers between muscles.

188 We found positive correlations between CSA and height, weight, and BMI supporting
189 the fact that muscle morphometry is associated to anthropometric features (Rezasoltani et al
190 1998). This could explain the CSA variability found in previous studies. In fact, the only
191 study investigating normative data of posterior cervical muscles reported that weight, rather
192 than gender, was a relevant cofounder factor for CSA (Rankin et al, 2005). Previous studies

193 investigating differences in CSA between neck pain patients and healthy subjects did not
194 control for the anthropometric variables (Fernández-de-las-Peñas et al, 2008; Kristjansson,
195 2004; Lee et al, 2007). De Pauw et al (2016) concluded that although there is evidence of
196 reduced CSA in the cervical multifidus in people with mechanical neck pain, more studies
197 are needed due to the inconsistency on the results. Future studies investigating differences
198 between pain populations and healthy subjects should include these considerations.

199 Finally, this study has some limitations. First, we included asymptomatic subjects.
200 We do not know if similar results would be observed in patients with mechanical neck pain
201 or WAD. Second, our sample was small. Therefore, our results should not be considered as
202 potential normative data, future studies are needed to determine muscle morphology data of
203 posterior neck muscles separately, e.g., semispinalis, splenius, multifidus, and rotators. In
204 addition, reliability of imaging capturing (probe assessment/patient positioning) was tested
205 within 10 minutes on the same day which may not be clinically relevant. Imaging capturing
206 reliability should ideally be assessed on different days in future studies. Finally, it is also
207 important to consider that fatty infiltration quantification is not possible with ultrasound
208 imaging and is currently possible with MRI, since MRI calculates the amount of fat by
209 differentiating fat and soft-aqueous tissue signal intensities (Elliott et al, 2013). Therefore,
210 RUSI should be only used for determining muscle morphology, e.g., CSA, size, or muscle
211 function, but not intramuscular quality, e.g., fat, or fibers.

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218 **Conclusions**

219 We found that ultrasound assessment of cervical multifidus at C4/C5 level is highly
220 reliable for evaluating CSA in asymptomatic people since imaging capturing and imaging
221 calculation exhibited excellent intra- and inter- examiner reliability. Reliability was similar
222 independently of the assessor experience. This paper proposes technical considerations for
223 future studies assessing muscle morphometry in neck pain populations.

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Legend of Figures

229 **Figure 1:** (A) Ultrasound probe placement over the cervical multifidus at C4 level; (B)
230 Ultrasound image showing the superficial posterior neck muscles.

231 **Figure 2:** Cross sectional area (CSA) assessment of the cervical multifidus. Borders were
232 marked as follows: 1, inferior limit: internal echogenic fascia between cervical multifidus
233 and rotator muscle; 2, superior limit: echogenic fascia between cervical multifidus and
234 semispinalis; 3, medial limit: echogenic spinous process

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Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of Cervical Multifidus Muscle in Healthy People: Imaging Capturing and Calculation Reliability Study

Highlights

1. Intra- and inter- examiner reliability of cervical multifidus imaging capturing and imaging calculation was excellent.
2. No significant differences between experienced and novice examiners and testers were found.
3. These values were obtained in asymptomatic individuals.

Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of Cervical Multifidus Muscle in Healthy People: Imaging Capturing and Imaging Calculation

Background: Studies have analyzed muscle morphometry of cervical multifidus by using ultrasound imaging, but its reliability is not clearly determined. **Objective:** To investigate intra- and inter-rater reliability of imaging capturing (probe assessment/patient positioning) and imaging calculation (scan assessment) of cervical multifidus cross sectional area (CSA) by considering the assessor's experience in asymptomatic individuals. **Design:** Reliability study. **Methods:** The CSA of C4/C5 cervical multifidus was assessed in 16 asymptomatic subjects. Two examiners performed the imaging capture and also repeated the procedure (probe placement/patient positioning) twice with a 10-min period between each. Other two raters conducted imaging calculations of CSA. Intra-examiner imaging capturing reliability, each rater (experienced and novice) calculated multifidus CSA of both images obtained by each examiner. Inter-examiner imaging capturing reliability, each rater calculated the CSA obtained by each examiner at the first imaging attempt. For imaging calculation reliability, each rater calculated multifidus CSA of all images captured by both examiners. Intra-class correlation coefficients (ICC) and standard error of measurement (SEM) were calculated. **Results:** Intra- (ICC_{3,1} 0.988-0.996, SEM 0.3%-0.7%) and inter- (ICC_{3,2} 0.958-0.965, SEM 2.6%-3.2%) examiner reliability of imaging capturing was excellent. Intra- and inter-rater reliability of imaging calculation was also excellent for both raters (experienced/novice). No differences between experienced or novice examiners or testers were found. **Conclusions:** This study found that intra- and inter-examiner/rater reliability of imaging capturing (probe assessment/ patient positioning) and imaging calculation (scan assessment) of the cervical multifidus CSA at C4/C5 level was excellent in asymptomatic subjects.

Key words: Rehabilitative ultrasound imaging, cervical multifidus, reliability.

Title Page

Title

Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of Cervical Multifidus Muscle in Healthy People: **Imaging Capturing and Imaging Calculation**

Authors

Juan A. Valera-Calero¹ PT, PhD candidate; Sandra Sánchez-Jorge² PT, PhD; Javier Álvarez-González³ PT, MSc; Ricardo Ortega-Santiago^{4,5} PT, PhD; Joshua A. Cleland^{6,7,8} PT, MSc, PhD; César Fernández-de-las-Peñas^{4,5} PT, PhD, DMSc; José L. Arias-Buría^{4,5} PT, MSc, PhD.

Affiliations

- (1) Escuela Internacional de Doctorado, Universidad Rey Juan Carlos, Alcorcón, Spain
- (2) Professional Practice, Madrid, Spain.
- (3) Servicio de Radiodiagnóstico. Hospital General Universitario Gregorio Marañón, Madrid, Spain.
- (4) Department of Physical Therapy, Occupational Therapy, Rehabilitation and Physical Medicine, Universidad Rey Juan Carlos, Alcorcón, Spain
- (5) Cátedra Institucional en Docencia, Clínica e Investigación en Fisioterapia: Terapia Manual, Punción Seca y Ejercicio Terapéutico, Universidad Rey Juan Carlos, Alcorcón, Madrid, Spain.
- (6) Department of Physical Therapy, Franklin Pierce University, Manchester, New Hampshire.
- (7) Rehabilitation Services, Concord Hospital, Concord, New Hampshire;
- (8) Manual Therapy Fellowship Program, Regis University, Denver, Colorado.

Address for reprint requests / corresponding author.

César Fernández de las Peñas
Facultad de Ciencias de la Salud
Universidad Rey Juan Carlos
Avenida de Atenas s/n
28922 Alcorcón, Madrid, SPAIN
E-mail address: cesar.fernandez@urjc.es

Telephone number: + 34 91 488 88 84

Fax number: + 34 91 488 89 57

1 Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound Imaging of
2 Cervical Multifidus Muscle in Healthy People: Imaging Capturing and
3 Imaging Calculation
4

5 **Abstract**

6 **Background:** Studies have analyzed muscle morphometry of cervical multifidus by using
7 ultrasound imaging, but its reliability is not clearly determined. **Objective:** To investigate
8 intra- and inter-rater reliability of imaging capturing (probe assessment/patient positioning)
9 and imaging calculation (scan assessment) of cervical multifidus cross sectional area (CSA)
10 by considering the assessor's experience in asymptomatic individuals. **Design:** Reliability
11 study. **Methods:** The CSA of C4/C5 cervical multifidus was assessed in 16 asymptomatic
12 subjects. Two examiners performed the imaging capture and also repeated the procedure
13 (probe placement/patient positioning) twice with a 10-min period between each. Other two
14 raters conducted imaging calculations of CSA. Intra-examiner imaging capturing reliability,
15 each rater (experienced and novice) calculated multifidus CSA of both images obtained by
16 each examiner. Inter-examiner imaging capturing reliability, each rater calculated the CSA
17 obtained by each examiner at the first imaging attempt. For imaging calculation reliability,
18 each rater calculated multifidus CSA of all images captured by both examiners. Intra-class
19 correlation coefficients (ICC) and standard error of measurement (SEM) were calculated.
20 **Results:** Intra- (ICC_{3,1} 0.988-0.996, SEM 0.3%-0.7%) and inter- (ICC_{3,2} 0.958-0.965, SEM
21 2.6%-3.2%) examiner reliability of imaging capturing was excellent. Intra- and inter-rater
22 reliability of imaging calculation was also excellent for both raters (experienced/novice).
23 No significant differences between experienced or novice examiners or testers were found.

24 **Conclusions:** This study found that intra- and inter-examiner/rater reliability of imaging
25 capturing (probe assessment/patient positioning) and imaging calculation (scan assessment)
26 of the cervical multifidus CSA at C4/C5 level was excellent in asymptomatic subjects.
27 **Key words:** Rehabilitative ultrasound imaging, cervical multifidus, reliability.

29 **Intra-rater and Inter-rater Reliability of Rehabilitative Ultrasound**
30 **Imaging of Cervical Multifidus Muscle in Healthy People: Imaging**
31 **Capturing and Imaging Calculation**
32

33 **Introduction**

34 Mechanical neck pain of insidious onset and whiplash associated disorders (WAD)
35 represent a major health care problem. While the general prognosis of neck pain is positive,
36 up to 50% of individuals continue reporting symptoms after 1-year (Kamper et al, 2008).
37 There is no consensus regarding the potential pathophysiology of neck disorders. One
38 mechanism may be related to the fact that neck pain induces changes in cervical muscle
39 performance. Several studies have reported that people with WAD show increased fatty
40 infiltrate and changes in cross sectional area (CSA) in the posterior cervical muscles,
41 specifically the multifidi (Abbott et al, 2015; Elliot et al, 2014; Snodgrass et al, 2019a).
42 However, most studies have used magnetic resonance imaging (MRI) to assess muscle
43 morphology (Owers et al, 2018), which is not readily available in clinical practice.

44 A more pragmatic method of measuring muscle morphology is ultrasonography; but
45 it its reliability must first be demonstrated (Whittaker et al, 2017). Some studies have
46 investigated the reliability of rehabilitative ultrasound imaging (RUSI) for examination of
47 the posterior neck muscles (Javanshir et al, 2010). Kristjansson (2004) analyzed the
48 reliability of assessing CSA of the C4 cervical multifidus and reported appropriate intra-
49 and inter-tester agreement in 10 asymptomatic subjects, and acceptable intra-, but
50 questionable inter-tester, agreement in 10 symptomatic subjects. Fernández-de-las-Peñas et
51 al (2008) reported excellent between-scan and good between-day assessment in individuals
52 with mechanical neck pain. Lee et al (2007) found that ultrasound imaging was as reliable
53 and valid as MRI for assessing cervical multifidus thickness after isometric contractions.

54 An important step before neck muscle composition can routinely be used in research
55 or clinical practice is establishing reliability of imaging calculation (scan assessment) but
56 also reliability of imaging capturing (patient positioning). This is particularly relevant since
57 ultrasonography is operator-dependent and the measurement protocol could influence the
58 imaging calculation. In fact, previous studies had mostly investigated the reliability of
59 imaging calculation (scan assessment) but not the reliability of imaging capturing (probe
60 assessment /patient repositioning). Further, reliability according to the experience of the
61 assessor has not been properly investigated. Our aim was to determine intra- and inter-
62 examiner/rater reliability of imaging calculation (scan/image assessment) and imaging
63 capturing (probe assessment/patient positioning) of cervical multifidus CSA considering
64 assessor experience

65

66 **Methods**

67 **Participants**

68 Asymptomatic volunteers without neck pain symptoms were recruited via local
69 announcements between December 2018 and June 2019. To be eligible to participate, they
70 had to be between 18 and 45 years old and with no history of neck pain the previous year.
71 Exclusion criteria included history of whiplash injury; any pharmacological treatment
72 affecting muscle tone, e.g., muscle relaxants, analgesics; prior history of cervical surgery;
73 cervical radiculopathy or myelopathy; presence of degenerative changes; and any medical
74 condition such as tumor or fracture. The study was approved by the Institutional Review
75 Ethical Committee of XX. All subjects signed the written informed consent prior to their
76 inclusion.

77 **Procedure Assessment - Imaging Capturing**

78 All images were acquired with a Toshiba Xario® 100 ultrasound equipment with a
79 PLU-1005 BT (7-15MHz) linear probe. Gain, frequency, depth, or focus were pragmatically
80 adapted by the examiner for each exam. Participants were placed in a prone position with
81 their arms in 90° abduction and the elbows flexed to 90°. The head/neck were stabilized
82 using the plinth's facial hole. A passive cranio-cervical flexion movement was performed
83 by the examiner to achieve a neutral position of the neck/head.

84 It has been estimated that measurements of C4 would exhibit less error (Lee et al,
85 2007); therefore, we assessed C4/C5 multifidus. To identify the cervical multifidus level,
86 the C2 spinous process was identified by palpation. At that point, the US probe was moved
87 caudally two segments until the posterior arch of C4 vertebra was visually identified. Then,
88 the transducer was moved lateral over the articular pillar (**Fig. 1A**). The image (scan) was
89 captured when the most superficial point of the spinous tubercle cortical surface and the
90 most superficial point of C4/C5 joint were visualized simultaneously (**Fig. 1B**).

91 **Measurement Assessment - Imaging Calculation**

92 Once the US image was captured, it was transferred to offline Oxyiri® Software for
93 calculating the CSA of the cervical multifidus by using on-screen calipers traced around the
94 following contours: 1, inferior limit: internal echogenic fascia between cervical multifidus
95 and rotator muscle (deep to cervical multifidus); 2, superior limit: echogenic fascia between
96 cervical multifidus and semispinalis; 3, medial limit: echogenic spinous process (**Fig. 2**).

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101 **Examiners**

102 A total of 4 examiners participated in the study. For imaging capturing, one experienced
103 (10 years of practice) and one novice (1 year of practice) examiner performed the patient
104 positioning/procedure placement and captured two images of the posterior neck muscles as
105 described. Each examiner repeated the assessment, twice with a 10-min period between.
106 Participants were repositioned on each assessment. On each assessment, an image of the
107 posterior neck muscles was obtained (Fig. 1B).

108 Another two examiners, identified in our study as raters, again one experienced and
109 the second novice (same experience as examiners) participated in the imaging calculation
110 of all images. Every image was coded to blind raters using alphanumeric codes. The order
111 of assessment and raters was numerically randomized between participants.

112 **Reliability Calculations**

113 We assessed the reliability of both imaging capturing and imaging calculation by
114 considering the examiner/rater experience. For imaging capturing intra-examiner reliability,
115 each rater (experienced/novice) calculated CSA of both images obtained by each examiner
116 (experienced/novice) at both assessments. For imaging capturing inter-examiner reliability,
117 each rater (experienced/novice) calculated the CSA of the image captured by each examiner
118 (experienced/novice) at the first positioning assessment.

119 For imaging calculation intra-rater reliability, each rater (experienced/novice) determined
120 the CSA of all images obtained by both examiners twice, one-week apart. For imaging
121 calculation inter-rater reliability, each rater (experienced/novice) calculated the CSA of all
122 images obtained by both examiners once.

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125 **Statistical Analysis**

126 Statistical analysis was performed using the SPSS package, Version 21 software for
127 Mac OS. Normal distribution of the data was verified by using the Shapiro-Wilk test. Intra-
128 and inter- examiner/rater reliability was estimated using 2-way mixed-model, consistency-
129 type intra class correlation coefficients (ICC). Reliability was classified as fair (ICC<0.50),
130 moderate (0.50<ICC<0.75), good (0.75<ICC<0.90) or excellent (ICC>0.90) (Koo and Li
131 2016). Standard error of measurement (SEM) was calculated using the resulting ICC values
132 and standard deviation (SD): $SEM (\%) = (SD \times \sqrt{1-ICC}) \times 100$ to assess measurement precision.
133 All tests were two-tailed with p-values <0.05 considered significant.

134

135 **Results**

136 From a total of 20 subjects responding to the announcement, 4 were excluded due to
137 previous whiplash injury (n=2) and history of neck pain the previous year (n=2). Sixteen
138 asymptomatic subjects (50% male) were finally included (total 64 images, n=4 per subject).
139 **Table 1** provides demographic features. Male exhibited higher anthropometric outcomes
140 and larger CSA than female (P<0.001). A positive correlation between multifidus CSA and
141 weight (r:0.473, P=0.006), height (r:0.385; P=0.03), and BMI (r:0.481, P=0.005) was found.

142 **Table 2** shows reliability data of imaging capturing. In general, imaging capturing
143 intra-examiner reliability (ICC_{3,1}) was excellent ranging from 0.988 to 0.996 with a SEM
144 from 0.3% to 0.7%. No difference between experienced/novice examiner/testers was found.
145 Inter-examiner reliability was also excellent for both experienced (ICC_{3,2} 0.965) and novice
146 (ICC_{3,2} 0.958) raters, with SEM of 2.6% and 3.2%, respectively.

147 Reliability data of imaging calculation of both raters is shown on **Table 3**. Again,
148 intra- and inter-rater reliability was excellent for both raters but with smaller SEM for intra-
149 rater reliability.

150

151 **Discussion**

152 This is the first study assessing reliability of both imaging capturing (positioning)
153 and imaging calculation (assessment) of the neck muscles considering the experience of the
154 assessor. In general, intra- and inter- rater reliability of imaging capturing and calculation
155 of cervical multifidus CSA was excellent when applied by an experienced or novice
156 assessor in asymptomatic individuals. Our findings are similar to those previously found in
157 patients with mechanical neck pain (Fernández-de-las-Peñas et al, 2008) and slightly better
158 than those previously reported by Kristjansson (2004). In addition, reliability data of
159 ultrasound imaging assessment was slightly superior to reliability data obtained for MRI.
160 Snodgrass et al (2019b) reported good to excellent intra- (ICC 0.78-0.96), but fair to good
161 inter- (ICC 0.44-0.88) rater reliability of cervical multifidus assessment using MRI in 5
162 asymptomatic individuals. Interestingly, no differences between an experienced and novice
163 examiner/rater were observed. This is a relevant topic since ultrasound imaging assessment
164 is operator-dependent. Two points are relevant for ultrasound assessment, probe angulation
165 and pressure. Whittaker et al (2009) showed that probe angulation of less than approx. 10
166 degrees, as it is commonly done in clinical practice, do not distort measurements of tissue
167 thickness. No data about probe pressure is available. It is possible that strict positioning and
168 measurement protocols followed in our study could explain high reliability values.

169 This study can help for developing specific protocols for image capturing and calculation
170 for both research and clinical practice. For instance, morphometry assessment, i.e., CSA, is
171 based on anatomical surrounding muscle contours. Previous studies recognized that lack of
172 proper visualization of the fascial layers dividing the cervical multifidus from surrounding
173 muscles (Fernández-de-las-Peñas et al, 2008; Kristjansson, 2004; Lee et al, 2007). One
174 potential reason for this lack of clarity of muscular fascial layers could be the presence of
175 fatty infiltration, a sign potentially associated with WAD (Owers et al, 2018). In the current
176 study, we assessed cervical multifidus, without including the rotators, as it was conducted
177 in previous studies (Fernández-de-las-Peñas et al, 2008; Kristjansson, 2004; Lee et al,
178 2007). The main reason was that the cervical multifidus attaches to the posterior aspect of
179 the facet capsules (Anderson et al, 2005) and play a relevant role in proprioception. In such
180 a scenario, fascial layers as border contours for determining muscle morphology may have
181 highly relevance. Since the current study included asymptomatic individuals, fascial layers
182 surrounding the multifidus were properly identified (Fig. 2). Rankin et al (2005) were not
183 able to consistently identify fascial divisions between multifidus/semispinalis and between
184 multifidus/rotators; therefore, they provided normative data of the whole muscle group and
185 not from individual muscles. It is also possible that technical improvements of ultrasound
186 imaging equipment, offering much better-definition and quality images, can also influence
187 proper visualization of fascial layers between muscles.

188 We found positive correlations between CSA and height, weight, and BMI supporting
189 the fact that muscle morphometry is associated to anthropometric features (Rezasoltani et al
190 1998). This could explain the CSA variability found in previous studies. In fact, the only
191 study investigating normative data of posterior cervical muscles reported that weight, rather
192 than gender, was a relevant cofounder factor for CSA (Rankin et al, 2005). Previous studies

193 investigating differences in CSA between neck pain patients and healthy subjects did not
194 control for the anthropometric variables (Fernández-de-las-Peñas et al, 2008; Kristjansson,
195 2004; Lee et al, 2007). De Pauw et al (2016) concluded that although there is evidence of
196 reduced CSA in the cervical multifidus in people with mechanical neck pain, more studies
197 are needed due to the inconsistency on the results. Future studies investigating differences
198 between pain populations and healthy subjects should include these considerations.

199 Finally, this study has some limitations. First, we included asymptomatic subjects.
200 We do not know if similar results would be observed in patients with mechanical neck pain
201 or WAD. Second, our sample was small. Therefore, our results should not be considered as
202 potential normative data, future studies are needed to determine muscle morphology data of
203 posterior neck muscles separately, e.g., semispinalis, splenius, multifidus, and rotators. In
204 addition, reliability of imaging capturing (probe assessment/patient positioning) was tested
205 within 10 minutes on the same day which may not be clinically relevant. Imaging capturing
206 reliability should ideally be assessed on different days in future studies. Finally, it is also
207 important to consider that fatty infiltration quantification is not possible with ultrasound
208 imaging and is currently possible with MRI, since MRI calculates the amount of fat by
209 differentiating fat and soft-aqueous tissue signal intensities (Elliott et al, 2013). Therefore,
210 RUSI should be only used for determining muscle morphology, e.g., CSA, size, or muscle
211 function, but not intramuscular quality, e.g., fat, or fibers.

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218 **Conclusions**

219 We found that ultrasound assessment of cervical multifidus at C4/C5 level is highly
220 reliable for evaluating CSA in asymptomatic people since imaging capturing and imaging
221 calculation exhibited excellent intra- and inter- examiner reliability. Reliability was similar
222 independently of the assessor experience. This paper proposes technical considerations for
223 future studies assessing muscle morphometry in neck pain populations.

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Legend of Figures

229 **Figure 1:** (A) Ultrasound probe placement over the cervical multifidus at C4 level; (B)
230 Ultrasound image showing the superficial posterior neck muscles.

231 **Figure 2:** Cross sectional area (CSA) assessment of the cervical multifidus. Borders were
232 marked as follows: 1, inferior limit: internal echogenic fascia between cervical multifidus
233 and rotator muscle; 2, superior limit: echogenic fascia between cervical multifidus and
234 semispinalis; 3, medial limit: echogenic spinous process

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Upper trapezius

◆
Splenius capitis

◆ 1
Semispinalis

◆
Multifidus

◆ 2
Rotators

◆ 3

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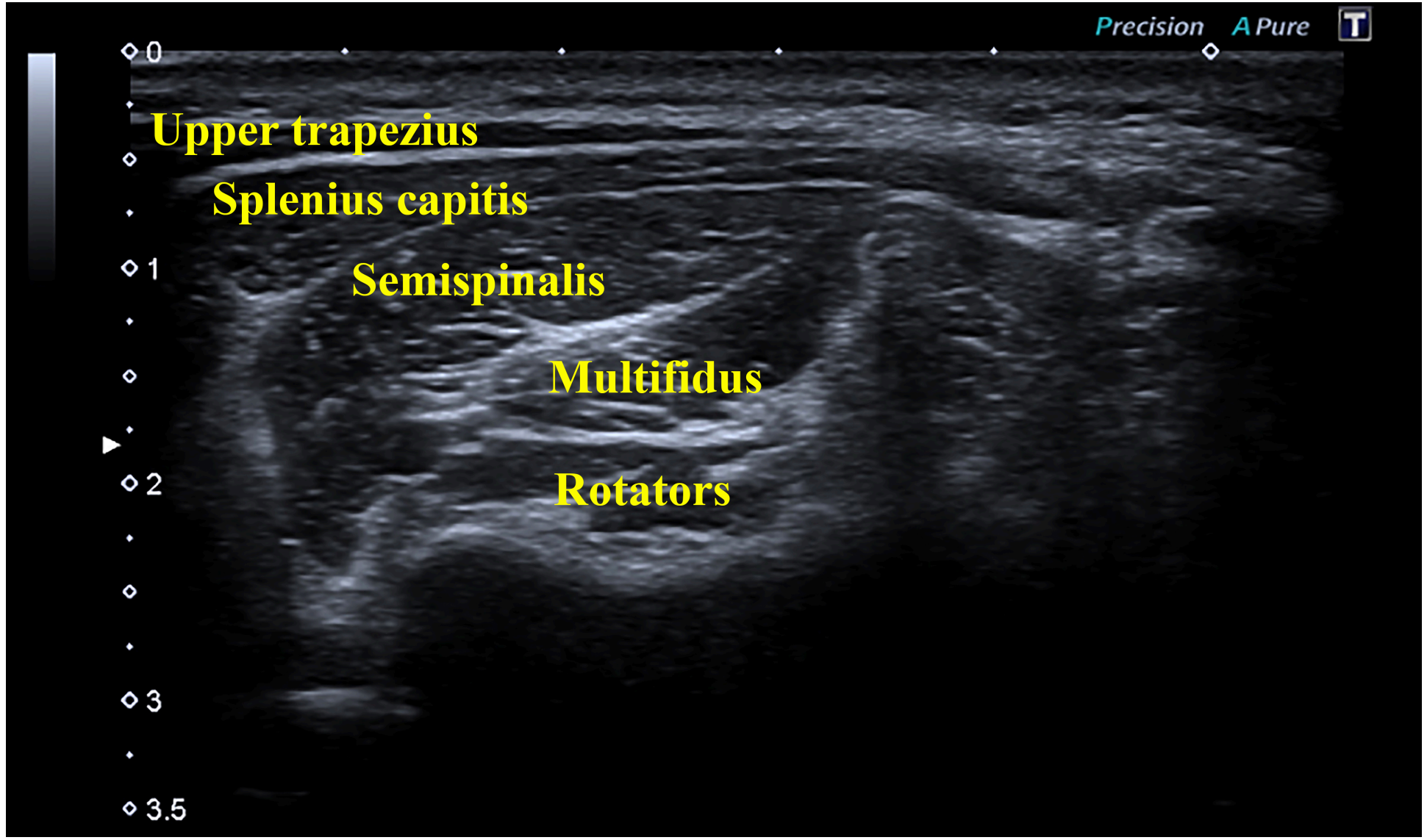


Figure 1B

Precision A Pure



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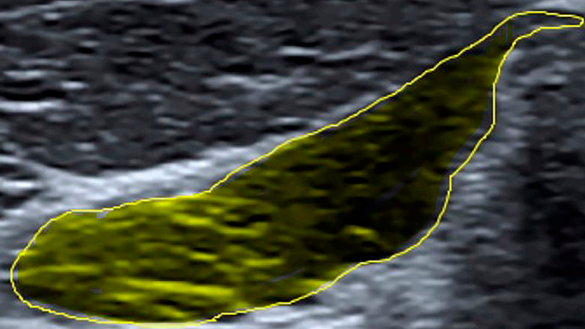


Table 1: Demographic Features of Participants by Gender

	Total (n=16)	Male (n=8)	Female (n=8)
Age (y)	28.5 (9.5)	31.0 (10.0)	25.5 (8.0)
Height (m)	1.70 (0.1)	1.80 (0.1)*	1.60 (0.1)
Weight (kg)	65.3 (15.0)	77.75 (9.0)*	53.0 (6.5)
BMI (kg/m ²)	21.9 (3.0)	23.78 (1.9)*	20.0 (1.9)
CSA right (cm ²)	1.30 (0.40)	1.50 (0.5)*	1.10 (0.3)
CSA left (cm ²)	1.20 (0.3)	1.40 (0.3)*	1.05 (0.15)

Values are expressed as means (SD)

* Significant differences between male and female (P<0.05)

Table 2: Intra- and Inter-Examiner Reliability of Imaging Capturing -
Probe Assessment/Patient Positioning

	ICC (95% CI)	SD (cm ²)	SEM
Intra-Examiner (ICC_{3,1}) Reliability (experienced)			
Experienced Rater	0.995 (0.989 - 0.997)	0.05	0.3%
Novice Rater	0.988 (0.976 - 0.994)	0.07	0.7%
Intra-Examiner (ICC_{3,1}) Reliability (novice)			
Experienced Rater	0.996 (0.992 - 0.998)	0.05	0.3%
Novice Rater	0.993 (0.985 - 0.996)	0.07	0.5%
Inter-Examiner Reliability (ICC_{3,2})			
Experienced Rater	0.965 (0.929 - 0.983)	0.14	2.6%
Novice Rater	0.958 (0.913 - 0.979)	0.16	3.2%

ICC: Intraclass Correlation Coefficient; SEM: Standard Error of Measurement
SD: Standard Deviation

Table 3: Intra- and Inter-Rater Reliability of Imaging Calculation –
Scan Assessment

	ICC (95% CI)	SD (cm ²)	SEM
Intra-rater Experienced Reliability (ICC _{3,1})	0.996 (0.994 - 0.997)	0.05	0.3%
Intra-rater Novice Reliability (ICC _{3,1})	0.938 (0.912 - 0.956)	0.18	4.4%
Inter-rater Reliability (ICC _{3,2})	0.922 (0.890 - 0.945)	0.21	5.8%

ICC: Intraclass Correlation Coefficient; SEM: Standard Error of Measurement
SD: Standard Deviation